

# Method and Apparatus for Cell Sorting

## BACKGROUND

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This application is related to and claims priority from United States provisional patent application number 60/420,351 filed Oct. 21, 2002 and hereby incorporates that application by reference.

### Field of the Invention

The present invention relates generally to the field of biological and medical instruments and more particularly to a method and apparatus for automatic cell sorting using gating technology.

### Description of the Prior Art

20 There is a large demand for cost effective cell sorting of stem and other cell types. Sorted isolated cell populations are used for transplantation into myeloablated cancer patients. There are currently about 100,000 such transplantations a year in the US. Cell sorting ideally  
25 needs to take place in a closed consumable container where hematopoietic stem and progenitor cell populations are sorted from peripheral blood, umbilical cord blood, and

bone marrow. However, current cell sorters require constant parameter adjustments, use open flow sorting technology which is susceptible to contamination and these sorters can cost in excess of \$250,000.

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Automated cell sorting techniques are becoming indispensable for both research and clinical applications. Typical prior art instruments interrogate the physical and chemical properties of cells followed by a physical  
10 separation of cells of interest at high speeds. The interrogations of each cell are done using optical techniques such as fluorescence followed by separation of the cells of interest using electrostatic or other physical separation methods. Conventional cell sorters utilize a  
15 single channel that operates at sorter rates of up to 60,000 cells per second. The sorting is done using an open fluid flow system that creates an aerosol environment.

There are several drawbacks to the prior art techniques: 1) the sorting rates cannot be much increased  
20 due to shear and pressure forces that damage the cells; 2) because separation takes place in an open fluid flow environment, there is a high potential for contamination; 3) the cost of current sorters is high.

What is badly needed is a cell sorter that operates in a closed flow environment (completely contained and isolated fluid system) that has intrinsic capability for very much faster sorting rates.

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#### SUMMARY OF THE INVENTION

The present invention relates to a cell sorter system for sorting desired cells from undesired matter which includes a precision pump for pumping cell-containing fluid  
10 into a detection and gating region and controlling positions of the cells in the detection and gating region; an optical detection system for determining when a desired cell is in a predetermined position in the detection and gating region; a select gate that can be magnetostrictive  
15 controlled, or otherwise controlled, that causes a desired cell to pass through a cell exit port and waste material to pass through a waste port according to an applied control signal or a magnetic field; and an optional vacuum system to cause the desired cell and/or waste to exit the correct  
20 ports.

The select gate, pump and detection system can be controlled by a microprocessor. Optical detection can be

based on fluorescence, scattered light or both. Both methods can be used simultaneously.

A magnetostrictive device is made from material that changes shape under an applied magnetic field. A  
5 magnetostrictive gate can be made from a monolithic or composite rod of magnetostrictive material that causes a valve to select a fluid channel between two or more ports (or an off-on situation using only one port). The rod can have any cross-section; however, cylindrical is preferred  
10 (Note: other structures besides rods will work). The control system can apply a magnetic field when flow through one of the ports is desired (for example, when a desired cell is in position). In the absence of any magnetic field, flow can take place through another port such as a  
15 waste port.

#### DESCRIPTION OF THE DRAWINGS

Fig. 1 shows a magnetostrictive capillary gating  
20 mechanism.

Fig. 2 shows a layout diagram of an optical detection system.

Fig. 3A shows a detail of optical coupling in and out  
of capillary tubes.

Fig. 3B is a side view of Fig. 3A.

Fig. 4A is a view of a fluidic micro-channel module.

5 Fig. 4B is a sectional view of the module from Fig.  
4A.

Several figures and drawings have been presented to  
better explain the present invention. The present  
10 invention is not limited to the embodiments or scope of the  
drawings.

#### **DESCRIPTION OF THE INVENTION**

The present invention relates to the use of  
15 magnetostrictive technology or other technology to create a  
cell sorter with a magnetostrictive gating mechanism (or  
any other high speed gating method). In a preferred  
embodiment, this gating mechanism utilizes a  
magnetostrictive rod coupled to a flow port selector  
20 component. Fig. 1 shows a magnetostrictive capillary  
gating mechanism. A magnetostrictive mini-rod 1 is  
mechanically connected to a ceramic or similar material  
flow selector 2 with a slot 3 that uncovers one of two, or

more, output ports 4 depending upon whether the mini-rod 1 is excited or un-excited by a magnetic field.

The mini-rod 1 is excited with a magnetic field that originates outside the capillary flow region. There needs  
5 to be no physical contact between the magnetic field generation means and the flow region. The mini-rod 1, by virtue of its magnetostriction property, physically expands when excited by an externally applied magnetic field. The flow selector 2 thus forms a valve between the ports 4 that  
10 can be very quickly and efficiently controlled with an external magnetic field.

The gating system of Fig. 1 can be exercised when a selected cell is in the correct position at the gate. Both ports 4 (or multiple ports) can have individual vacuum  
15 sources coupled to them so that the opening of one of the ports allows the cells of interest to be moved (removed) by a combination of suction and flow dynamics. Once the cells of interest are removed, the magnetic field can also be removed, and the gating port allowed to re-align with the  
20 other (or one of the other) ports for normal waste flow exit.

Fluid is caused to flow into the system from a precision fluid pump into an input channel or capillary 5

that can be around 40 micrometers in diameter. The capillary 5 ends at the selection device 2. Fig. 1 shows the device in the normal position where a cell has not been selected for removal. The speed of the fluid flow from the pump can normally be high, and when a cell needs to be removed, the pump speed can be reduced and carefully synchronized to the selection port. When a cell needs to be removed, the fluid pump can be stopped, the gate moved to the remove position, the pump moved for one cell removal, and then the gate moved back to its normal closed position. A typical magnetostrictive rod is capable of moving around 1000 parts per million or around 1 micron per millimeter. For a movement of 25-30 microns, a rod of this type would need to be around 25-30 mm long. Any rod of any material that can expand is within the scope of the present invention. The gating device shown in Fig. 1, using a magnetostrictive rod, is capable of operating at speeds up to 10,000 Hz.

The system shown in Fig. 1 is coupled fluid-wise to a precision dispensing pump. The pump system should be capable of making precise micro-displacements of at least 0.5 micron resolution to obtain maximum accuracy. The pump system is capable of removing large volumes of aphaeresis

material, and then slowing feeding the material to the  
input capillary channel or channels 5. The fluid is  
generally moved to the capillary tube in discrete movements  
that are usually synchronized to an optical detection  
5 system and the cell gating system shown in Fig. 1.  
Continuous flow systems are within the scope of the present  
invention.

The overall cell sorter system couples the action of a  
precision pump, an optical detection system and a sorting  
10 gate mechanism such as is shown in Fig.1. Fig. 2 shows an  
embodiment of an optical detection system that is could be  
used with the present invention. An argon 488 nm laser 6  
acts as a fluorescence source while a helium neon 633 nm  
laser 7 acts as a light scatter source. The two lasers are  
15 coupled into a mixing rod 8 that is used to combine the  
source wavelengths and effectively couple light into fibers  
9. The light fibers 9 are used to bring light into  
capillary cells 10. Pairs of other fibers 11 are used to  
couple fluorescence and light scatter from each capillary  
20 cell into multi-channel array detectors 12. The multi-  
channel array detectors 12 can contain photo-multipliers or  
diode arrays or any other light detection means. Any other



type of optical system or combination of wavelengths is within the scope of the present invention.

The fiber optics 11 can be positioned as shown in Figs. 3A and 3B where each capillary is positioned so that  
5 the optics for the source and detector are 180 degrees apart. Fluorescence detection can have its fibers one above another as shown in Figs. 3A and 3B. The capillary detection modules can be round or square and can use optical refractive index matching fluids for coupling into  
10 the output fibers (or lens/fibers). Figs. 3A and 3B show the capillary tubes 10 from a top view (Fig. 3A) and a side view (Fig. 3B). A Fluorescence and light scatter source 12 feeds the light of two different wavelengths into the capillaries 10. Fluorescence detection 13 and light  
15 scatter detection 14 can be positioned 90 degrees apart as shown in Figs. 3A and 3B. The embodiments shown in Figs. 3A and 3B are representative of the types that can be used with the present invention. The present invention includes many other embodiments of optical detection.

20 When either a fluorescence or light scatter signal (or both) indicates a cell to be sorted is in position, the pump control electronics keeps track of the time shift necessary so that the cells are properly presented to the

gating mechanism. The gating mechanism can be exercised when the selected cell is in exactly the correct position. Both ports under the gating mechanism can have a vacuum source coupled to them. The opening of the proper port  
5 causes the selected cell to exit (be removed) through the correct channel. One exit channel could be for selected cells and the other for all else. Multiple channels (more than two) are within the scope of the present invention and can lead to more sophisticated sorting based on various  
10 cell properties.

When a selected cell is in position in the capillary, the control electronics either applies the external magnetic field, or not, depending upon which exit port is desired. Once the magnetic field is removed (if it had  
15 been applied), the gate re-aligns itself to the normal position or non-selected (waste) port. The speed of fluid flow from the pump can be high as previously discussed. When a cell needs to be removed, the flow speed can be reduced and carefully synchronized to the gate. Continuous  
20 flow systems are within the scope of the present invention.

Figs. 4A and 4B show an embodiment of a fluidic micro-channel module that can be laser machined with an Eximer laser on a ceramic or polymer (or any other suitable

material) substrate. A fluid inlet port 14 can be part of a laser machined micro-channel plate 15. The fluid inlet port 14 leads to fluorescence and scattered light channel 16 and on to a flow selector component or gate 17 and on to an cell collector port 18 and a waste port 19. A magnetotriactive rod 20 is shown attached to the flow selector 17 such that when it experiences an applied magnetic field, it changes the flow from the waste port 19 to the cell collector port 18. As stated before, the control electronics causes the magnetic field to be applied (or not applied) to choose one of the ports just when the cell is in the correct position. The sensor for the cell position can be the fluorescence or scattered light detectors external to the module shown in Figs. 4A and 4B.

15       The present invention thus couples a precision pump, an optical cell detection system and a control channel into a closed system that can move a cell into position to be identified, identify it and make a sort decision, move the selected cell to the control gate (if not already in position), set the control gate, and pull the selected cell out into a proper exit port. The present invention can be run in a pulsed (or discrete motion) mode, or it can be run with continuous flow and hence continuous cell motion.

Cells are identified and classified by the optical detection system according to optical properties that are either intrinsic or can be given to the desired cells through methods well-known in the art.

5       The present invention allows cells to be sorted by using a dynamic gate that can be constructed using magnetostrictive or other technology to create a small capillary valve. The valve can be switched from one state to another by the application of a magnetic field. The  
10 valve can be constructed where two (or more) ports are very close together so that as one port closes, the other is opening, or it can be constructed with ports further apart so that there is a period of time when both ports are blocked. The valve system can be part of a single or  
15 multiple capillary block. Such a block can be micro-machined using laser technology. The fluid flow through the present invention can be pulsed or continuous. Cells and other material can be sucked out of ports using an optional vacuum system on each port. Cell detection can be  
20 accomplished using either fluorescence or scattered light, or both simultaneously. The system can be controlled by a single or by multiple microprocessors.

The present invention has been described by written descriptions and figures. A person skilled in the art will realize that many changes and variations can be made that are still within the scope of the present invention.

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